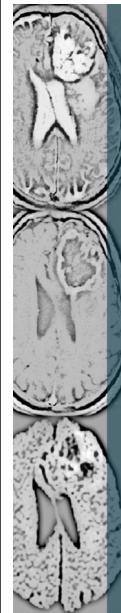




## 磁振影像學MRI 重複時間與回波時間 TR & TE

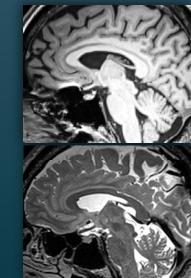
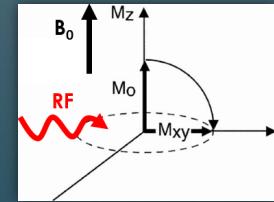
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## Procedure of MRI

- Alignment (magnetization)  $B_0$
- Precession  $\omega_0 = \gamma B_0$
- Resonance (given  $B_1$  by RF with  $\omega_2$ )  $\omega_1 = \gamma B_1$ ,  $B_1 \perp B_0$ 
  - The most effective resonance is produced when  $\omega_0 = \omega_2$
- MR signal (EMF, relaxation time )
- Imaging (Pulse sequencing)
  - Tissue Contrast: Image weighting
  - Spatial localization: Spatial Encoding



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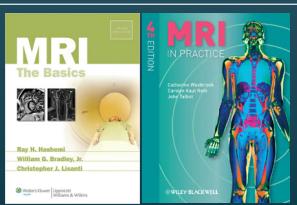
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## 本週課程內容 <http://cflu.lab.nycu.edu.tw>

- 重複時間與回波時間(TR & TE)
- TR&TE綜合效應(T1/T2權重)

- MRI The Basics (3rd edition)
  - Chapter 5: TR, TE, and Tissue Contrast
- MRI in Practice, (4th edition)
  - Chapter 2: Image Weighting and Contrast



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## 重複時間與回波時間TR, TE

Time of Repetition (TR) & Time of Echo (TE)  
Repetition Time (TR) & Echo Time (TE)

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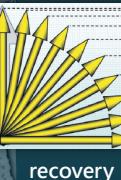
## T1 & T2 Relaxation Time

T1:  
The **longitudinal** relaxation time  
The **spin-lattice** relaxation time

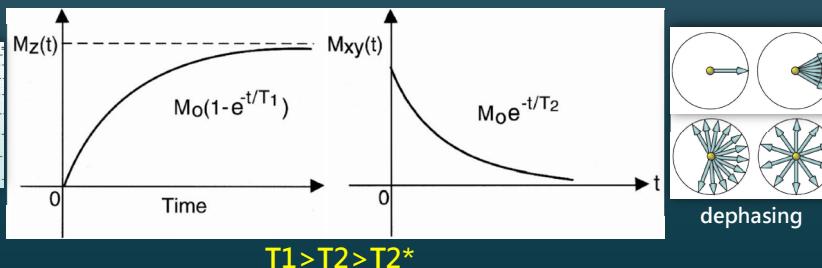
$$M_z(t) = M_0(1 - e^{-t/T_1})$$

T2:  
The **transverse** relaxation time  
The **spin-spin** relaxation time

$$M_{xy}(t) = M_0 e^{-t/T_2}$$



recovery



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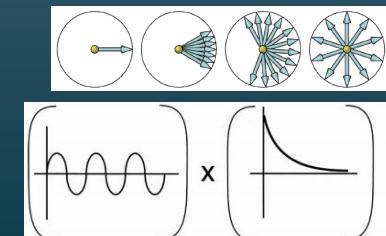
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## Received Signal: Free Induction Decay

The oscillating, decaying signal is called an **FID**.

$$M_{xy}(t) = M_0 e^{-t/T_2^*} (\cos \omega_0 t)$$



The frequency of the received signal is also  $\omega_0$ .

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## T1, T2 $\Leftrightarrow$ TR, TE

- T1 and T2 are inherent properties of the tissue and therefore fixed.
- TR and TE can be controlled and adjusted by the operator.
- By appropriate setting of TR and TE, we can put more "weight" on T1 or T2.

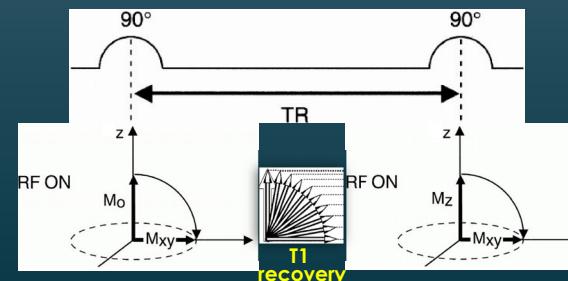
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## TR (Repetition Time)

- To **spatially encode** the signal and to **increase the signal-to-noise ratio**, we have to apply the RF pulse **multiple times** while varying the gradients.
- The time interval between RF pulses is called TR.



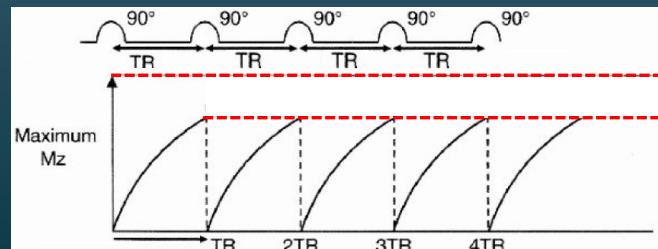
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## T1 Recovery During Successive 90° Pulses

- $M_z(TR) = M_0(1 - e^{-TR/T1})$ 
  - If  $TR \rightarrow \infty$ ,  $M_z(TR) = M_0$
  - Otherwise,  $M_z(TR) < M_0$



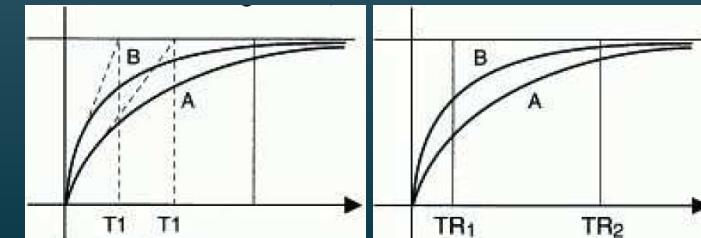
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## Tissue Contrast (T1 weighting)

- If tissue A has a longer T1 than tissue B, it takes longer to recover  $M_z$ .
- Shorter TR ( $TR_1$ ) offers better T1 tissue contrast (difference) between tissues A and B.
- **Longer TR reduces the T1 weighting(contrast).**



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## Tissue Contrast (T1 weighting)

- **Longer TR reduces the T1 weighting(contrast).**
- We can certainly minimize the T1 effect with a TR of 2000 to 3000 msec.
- In general, if TR is 4 to 5 times T1, then the T1 effect becomes negligible.
- Ideally, we use  $TR=T1$  for T1-weighted imaging.

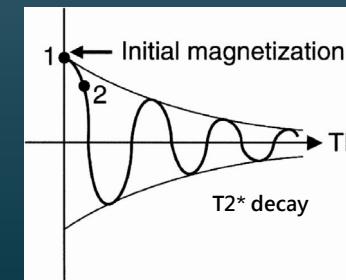
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## TE (Time to Echo or Echo Delay Time)

- We wait a short period of time (TE) after RF pulse and then make the measurement.
- The  $T2^*$  decay curve (FID) starts out at the value of  $M_0(1 - e^{-TR/T1})$  on the T1 recovery curve and then decays very quickly.



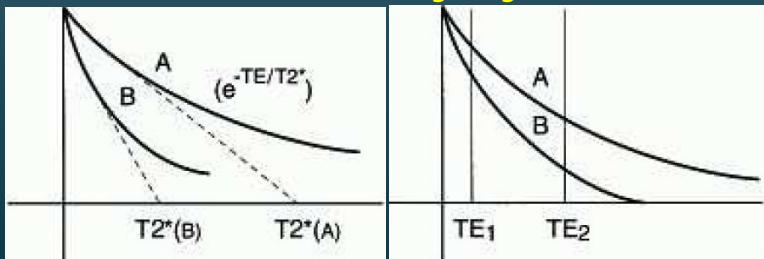
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## Tissue Contrast (T2\* weighting)

- If tissue A has a longer T2\* than tissue B, it takes longer to decay  $M_{xy}$ .
- Longer TE ( $TE_2$ ) offers better T2\* tissue contrast (difference) between tissues A and B.
- Shorter TE reduces the T2\* weighting(contrast).**



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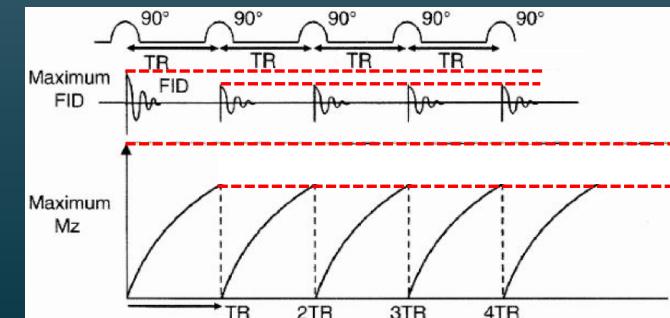
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## FID During Successive 90° Pulses

- The FID signal (the voltage of EMF) would be proportional to

$$M_0(1-e^{-TR/T1}) e^{-TE/T2*}$$



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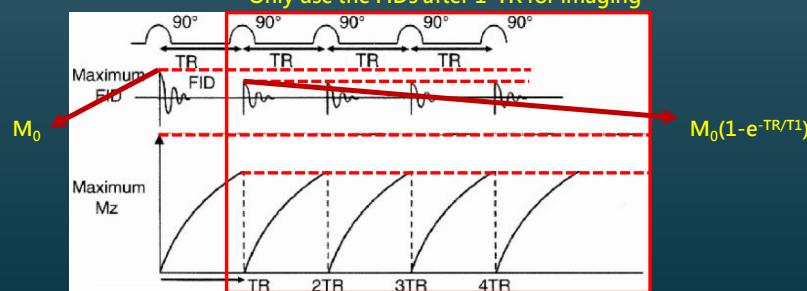
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## Dummy Scans

- Each dummy scan contains all of the RF pulses, delays and gradients used in the pulse program.
- But the receiver is not turned on to collect data.
- To ensure that the spin system is in a steady state.

Only use the FIDs after 1\*TR for imaging



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## TR&TE綜合效應(T1/T2權重)

T1 or T2 Weighting

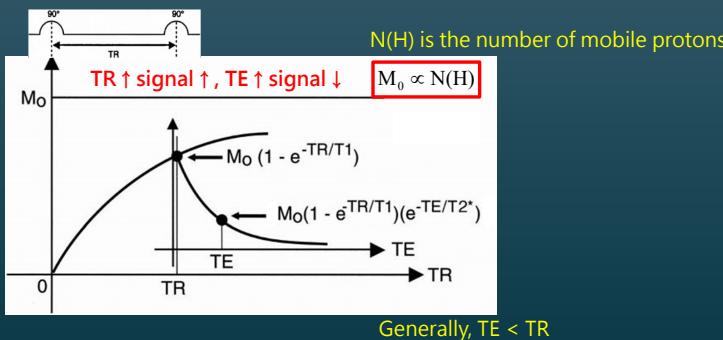
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## Combination of TR and TE

- Don't forget that the FID is originated from  $M_{xy}$



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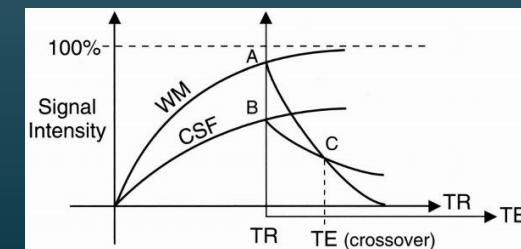
## Exercise 5-1

- (a) For a  $TR = 2000$  msec, find the relative signal intensities for WM and CSF (i.e., points A and B on the graph).

$$\begin{aligned} \text{WM: } 100(1 - e^{-2000/500}) &= 100(1 - 0.018) = 98.2 \\ \text{CSF: } 100(1 - e^{-2000/2000}) &= 100(1 - 0.368) = 63.2 \end{aligned}$$

Assume...

	T1 (msec)	T2 (msec)	N(H)
WM	500	100	100
CSF	2000	200	100



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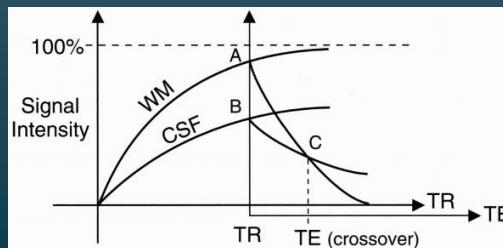
## Exercise 5-1

- (b) Calculate the crossover TE where WM and CSF have identical T2 weighting (point C).

$$\begin{aligned} 98.2(e^{-TE/100}) &= 63.2(e^{-TE/200}) \\ 98.2 &= 63.2 \frac{e^{-TE/200}}{e^{-TE/100}} \\ \frac{98.2}{63.2} &= \frac{e^{-TE/200}}{e^{-TE/100}} \\ \ln(1.55) &= (-TE/200) - (-TE/100) \\ 0.4407 &= TE/200 \\ TE &= 88.14 \end{aligned}$$

Assume...

	T1 (msec)	T2 (msec)	N(H)
WM	500	100	100
CSF	2000	200	100



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## Exercise 5-1

- (c) Now, calculate the signal ratio of CSF/WM for TE = 25 (first echo) and TE = 100 msec (second echo).

$$\begin{aligned} \text{WM: } 100(1 - e^{-2000/500})(e^{-100/100}) &= 98.2 \times 0.78 = 76.6 \\ \text{CSF: } 100(1 - e^{-2000/2000})(e^{-25/200}) &= 63.2 \times 0.88 = 55.6 \end{aligned}$$

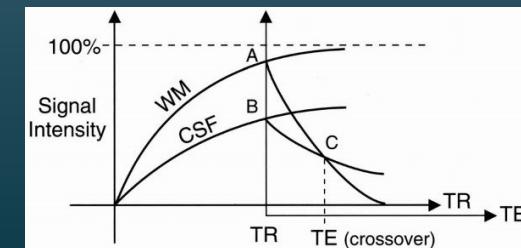
$$\text{CSF/WM} = 0.72$$

$$\begin{aligned} \text{WM: } 100(1 - e^{-2000/500})(e^{-100/100}) &= 98.2 \times 0.37 = 36.3 \\ \text{CSF: } 100(1 - e^{-2000/2000})(e^{-100/200}) &= 63.2 \times 0.61 = 38.6 \end{aligned}$$

$$\text{CSF/WM} = 1.06$$

Assume...

	T1 (msec)	T2 (msec)	N(H)
WM	500	100	100
CSF	2000	200	100



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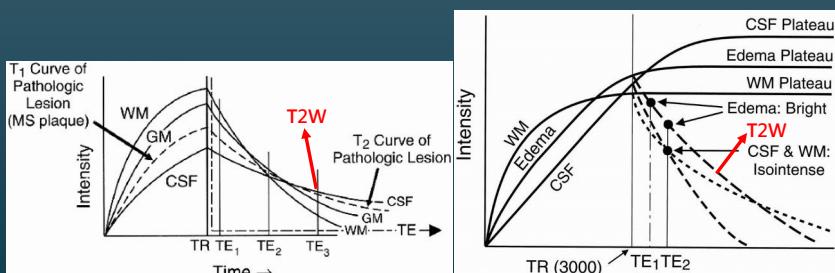
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## Differentiate abnormality

- Adjust T1/T2 weighting to enhance abnormalities.



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## Intracranial Hemorrhage on MRI

Staging	Time	Component	T1W	T2W
Hyperacute	1 day			
Acute	1-3 days	oxyhemoglobin	hypointense	hyperintense
Subacute _ early	3-7 days	deoxyhemoglobin	isointense	hypointense
Subacute _ late	1-3 weeks	methemoglobin(intracellular)	hyperintense inner : hypointense outer : hyperintense	
Chronic _ early	3 weeks - months	methemoglobin(extracellular)	hyperintense	hyperintense
Chronic _ late	months - years	hemochrome	hypointense	hypointense or isointense
Remote	months - years	hemosiderin/ferritin	hypointense	hyperintense

<http://lib.yeezen.com.tw/lb/Radiology/gloo/n-mrihemorrhage.html>

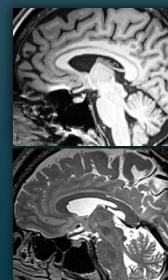
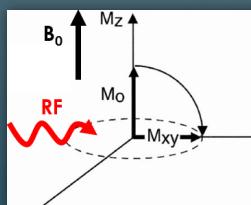
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THE END

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