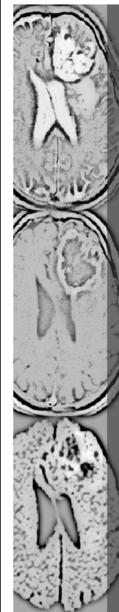




磁振影像學MRI 重複時間與回波時間 TR & TE

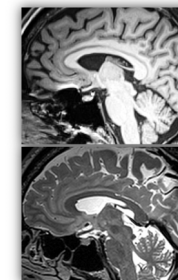
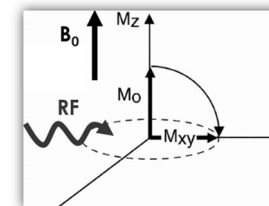
盧家鋒 副教授

國立陽明交通大學
生物醫學影像暨放射科學系
alvin4016@nycu.edu.tw



Procedure of MRI

- Alignment (magnetization) B_0
- Precession $\omega_0 = \gamma B_0$
- Resonance (given B_1 by RF with ω_2) $\omega_1 = \gamma B_1$, $B_1 \perp B_0$
 - The most effective resonance is produced when $\omega_0 = \omega_2$
- MR signal (EMF, relaxation time)
- Imaging (Pulse sequencing)
 - Tissue Contrast: Image weighting
 - Spatial localization: Spatial Encoding



<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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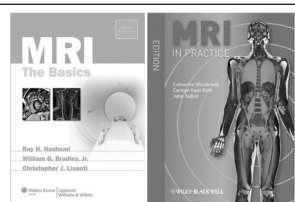
2



本週課程內容 <http://cflu.lab.nycu.edu.tw>

- 重複時間與回波時間(TR & TE)
- TR&TE綜合效應(T1/T2權重)

- MRI The Basics (3rd edition)
 - Chapter 5: TR, TE, and Tissue Contrast
- MRI in Practice, (4th edition)
 - Chapter 2: Image Weighting and Contrast



<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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重複時間與回波時間TR, TE

Time of Repetition (TR) & Time of Echo (TE)
Repetition Time (TR) & Echo Time (TE)

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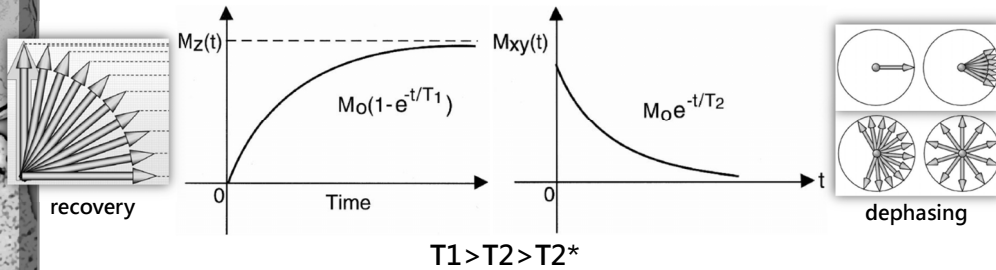
T1 & T2 Relaxation Time

T1:
The longitudinal relaxation time
The spin-lattice relaxation time

$$M_z(t) = M_0(1 - e^{-t/T1})$$

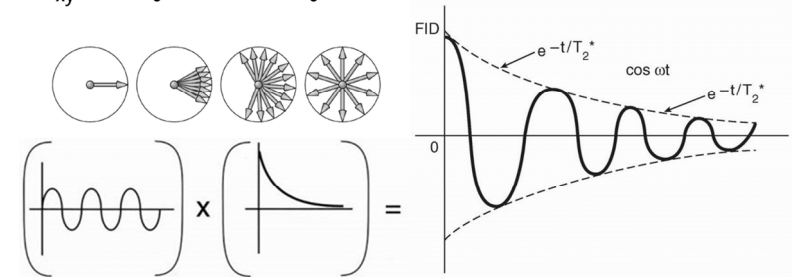
T2:
The transverse relaxation time
The spin-spin relaxation time

$$M_{xy}(t) = M_0 e^{-t/T2}$$



Received Signal: Free Induction Decay

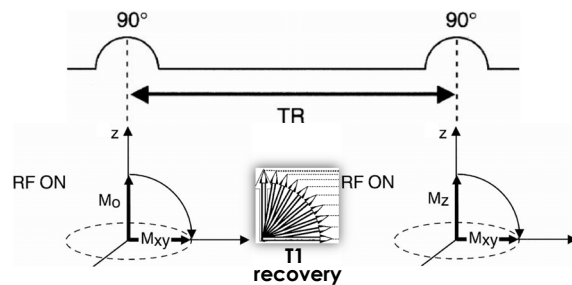
- The oscillating, decaying signal is called an FID.
- $M_{xy}(t) = M_0 e^{-t/T2^*} (\cos \omega_0 t)$



The frequency of the received signal is also ω_0 .

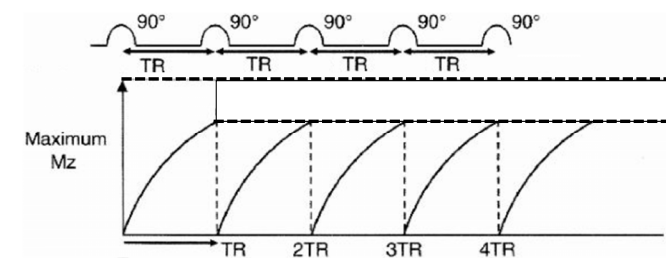
TR (Repetition Time)

- To spatially encode the signal and to increase the signal-to-noise ratio, we have to apply the RF pulse *multiple times* while varying the gradients.
- The time interval between RF pulses is called TR.



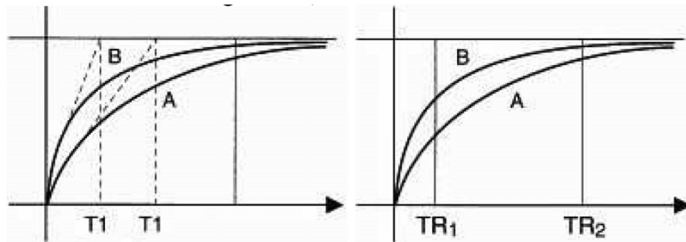
T1 Recovery During Successive 90° Pulses

- $M_z(TR) = M_0(1 - e^{-TR/T1})$
 - If $TR \rightarrow \infty$, $M_z(TR) = M_0$
 - Otherwise, $M_z(TR) < M_0$



Tissue Contrast (T1 weighting)

- If tissue A has a longer T1 than tissue B, it takes longer to recover M_z .
- Shorter TR (TR_1) offers better T1 tissue contrast (difference) between tissues A and B.
- **Longer TR reduces the T1 weighting(contrast).**



<http://cflu.lab.nyu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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Tissue Contrast (T1 weighting)

- **Longer TR reduces the T1 weighting(contrast).**
- We can certainly minimize the T1 effect with a TR of 2000 to 3000 msec.
- In general, if TR is 4 to 5 times T1, then the T1 effect becomes negligible.
- Ideally, we use $TR \approx T1$ for T1-weighted imaging.

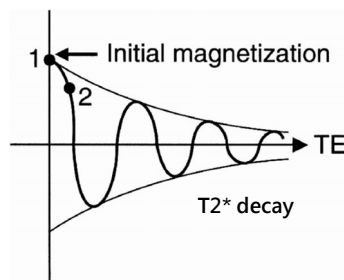
<http://cflu.lab.nyu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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TE (Time to Echo or Echo Delay Time)

- We wait a short period of time (TE) after RF pulse and then make the measurement.
- The $T2^*$ decay curve (FID) starts out at the value of $M_0(1 - e^{-TR/T1})$ on the T1 recovery curve and then decays very quickly.



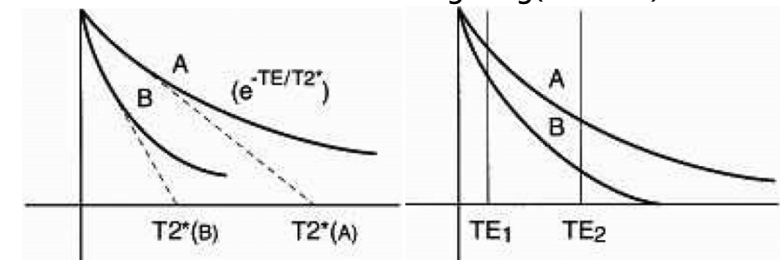
<http://cflu.lab.nyu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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Tissue Contrast ($T2^*$ weighting)

- If tissue A has a longer $T2^*$ than tissue B, it takes longer to decay M_{xy} .
- Longer TE (TE_2) offers better $T2^*$ tissue contrast (difference) between tissues A and B.
- **Shorter TE reduces the $T2^*$ weighting(contrast).**



<http://cflu.lab.nyu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

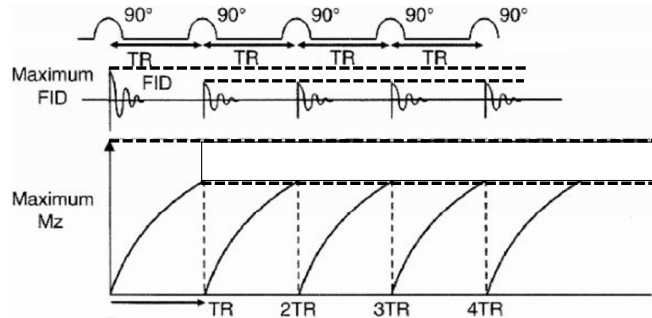
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FID During Successive 90° Pulses

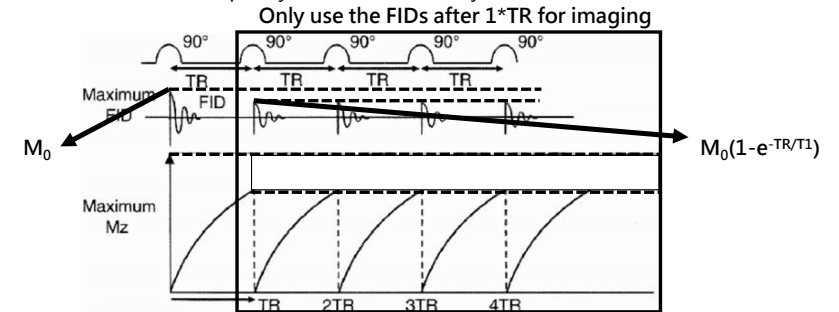
- The FID signal (the voltage of EMF) would be proportional to

$$M_0(1 - e^{-TR/T1}) e^{-TE/T2^*}$$



Dummy Scans

- Each dummy scan contains all of the RF pulses, delays and gradients used in the pulse program.
- But the receiver is not turned on to collect data.
- To ensure that the spin system is in a steady state.



TR&TE綜合效應(T1/T2權重)

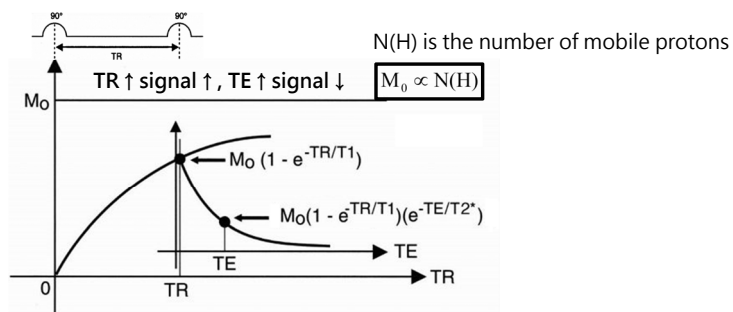
T1 or T2 Weighting

T1, T2 ⇔ TR, TE

- T1 and T2 are inherent properties of the tissue and therefore fixed.
- TR and TE can be controlled and adjusted by the operator.
- By appropriate setting of TR and TE, we can put more "weight" on T1 or T2.

Combination of TR and TE

- Don't forget that the FID is originated from M_{xy}



Exercise 5-1

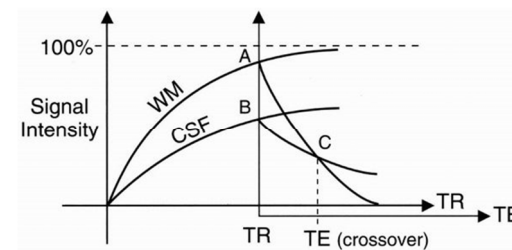
- (a) For a $TR = 2000$ msec, find the relative signal intensities for WM and CSF (i.e., points A and B on the graph).

Assume...

	T1 (msec)	T2 (msec)	N(H)
WM	500	100	100
CSF	2000	200	100

$$\text{WM: } 100(1 - e^{-2000/500}) = 100(1 - 0.018) = 98.2$$

$$\text{CSF: } 100(1 - e^{-2000/2000}) = 100(1 - 0.368) = 63.2$$



Exercise 5-1

- (b) Calculate the crossover TE where WM and CSF have identical T2 weighting (point C).

Assume...

	T1 (msec)	T2 (msec)	N(H)
WM	500	100	100
CSF	2000	200	100

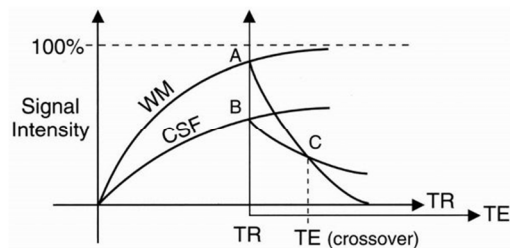
$$98.2(e^{-TE/100}) = 63.2(e^{-TE/200})$$

$$\frac{98.2}{63.2} = \frac{e^{-TE/200}}{e^{-TE/100}}$$

$$\ln(1.55) = (-TE/200) - (-TE/100)$$

$$0.4407 = TE/200$$

$$TE = 88.14$$



Exercise 5-1

- (c) Now, calculate the signal ratio of CSF/WM for $TE = 25$ msec (first echo) and $TE = 100$ msec (second echo).

Assume...

	T1 (msec)	T2 (msec)	N(H)
WM	500	100	100
CSF	2000	200	100

$$\text{WM: } 100(1 - e^{-2000/500})(e^{-25/100}) = 98.2 \times 0.78 = 76.6$$

$$\text{CSF: } 100(1 - e^{-2000/2000})(e^{-25/200}) = 63.2 \times 0.88 = 55.6$$

$$\text{CSF/WM} = 0.72$$

$$\text{WM: } 100(1 - e^{-2000/500})(e^{-100/100}) = 98.2 \times 0.37 = 36.3$$

$$\text{CSF: } 100(1 - e^{-2000/2000})(e^{-100/200}) = 63.2 \times 0.61 = 38.6$$

$$\text{CSF/WM} = 1.06$$

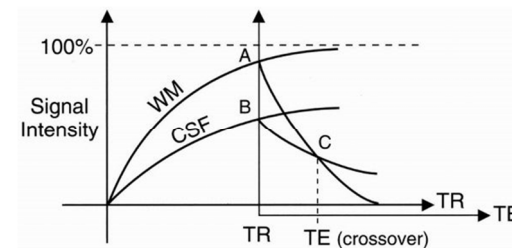


Image Contrast

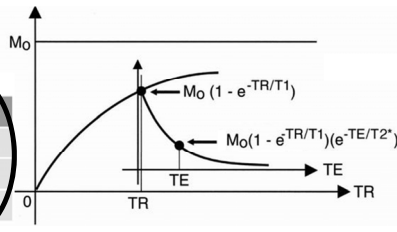
- Long TR, short TE → proton density
- Long TR, long TE → T2*-weighted
- Short TR, short TE → T1-weighted
- Short TR, long TE → no signal

Example:
 Long TR 2000 ms
 Short TR 300-700 ms
 Long TE 60 ms+
 Short TE 10-25 ms

Table 2.3 Parameters used in gradient echo.

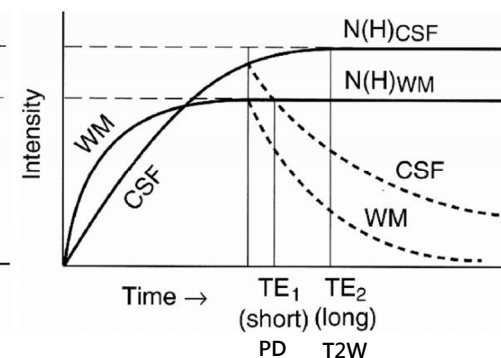
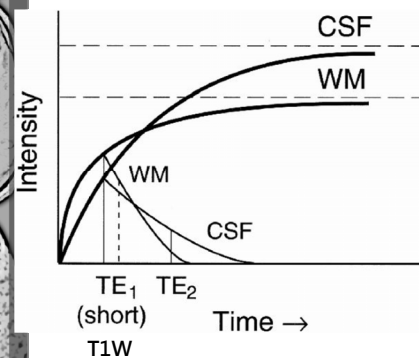
Weighting	TR	TE
T1	short	short
T2	long	long
Proton density	long	short

Flip angle
 large
 small
 small



Tissue Contrast

- Shorter TR vs. Longer TR

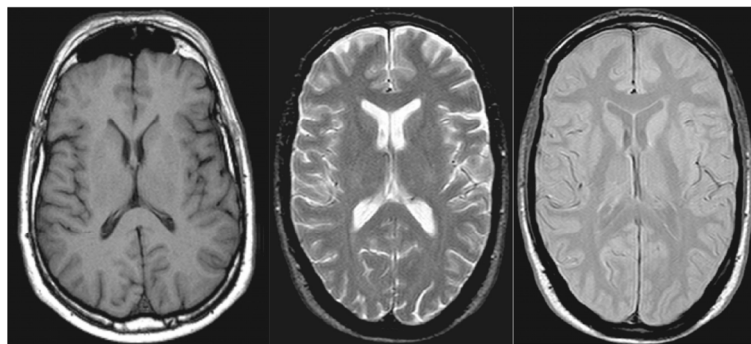


T1/T2/PD weighted Images

T1W

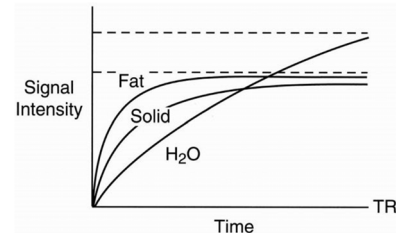
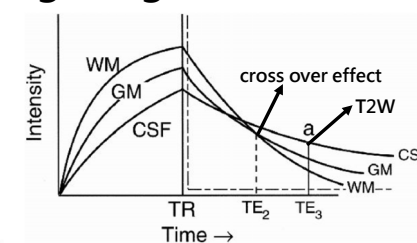
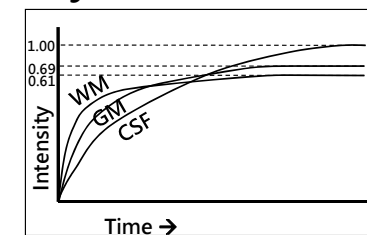
T2W

PDW



CSF > edema > GM > WM

Adjust T1 and T2 weighting

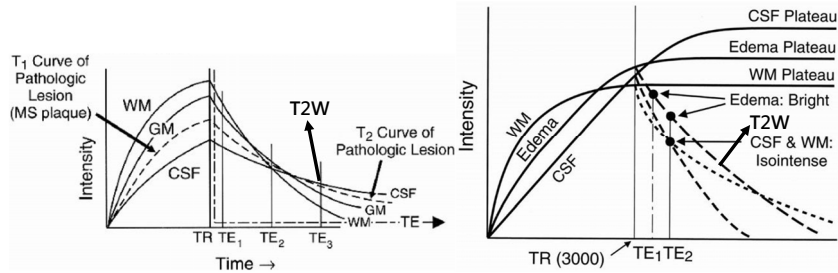


T1: CSF > GM > WM
 T2: CSF > GM > WM
 N(H): CSF > GM > WM

T1: H₂O > Solid tissue > Fat
 T2: H₂O > Fat > Solid tissue
 N(H): H₂O > Fat > Solid tissue

Differentiate abnormality

- Adjust T1/T2 weighting to enhance abnormalities.



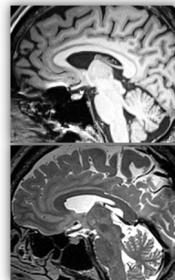
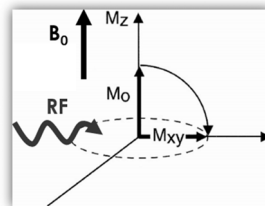
Intracranial Hemorrhage on MRI

Staging	Time	Component	T1W	T2W
Hyperacute	1 day			
Acute	1-3 days	oxyhemoglobin	hypointense	hyperintense
Subacute_early	3-7 days	deoxyhemoglobin	isointense	hypointense
Subacute_late	1-3 weeks	methemoglobin(intracellular)	hyperintense	inner :hypointense
				outer : hyperintense
Chronic_early	3weeks - months	methemoglobin(extracellular)	hyperintense	hyperintense
Chronic_late	months - years	hemosiderin	hypointense	hyperintense or isointense
Remote	months - years	hemosiderin/ferritin	hypointense	hyperintense

<http://lib.yeezen.com.tw/lb/Radiology/gloo/n-mrihemorrhage.html>

Procedure of MRI

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- Precession $\omega_0 = \gamma B_0$
- Resonance (given B_1 by RF with ω_2) $\omega_1 = \gamma B_1$, $B_1 \perp B_0$
 - The most effective resonance is produced when $\omega_0 = \omega_2$
- MR signal (EMF, relaxation time)
- Imaging (Pulse sequencing)
 - Tissue Contrast: Image weighting
 - Spatial localization: Spatial Encoding



THE END

alvin4016@nycu.edu.tw

Intracranial Hemorrhage on MRI

Stage	Time	Hemoglobin	T1	T2
Hyperacute	< 24 hours	Oxyhemoglobin	Iso	Hyper
Acute	1 - 3 days	Deoxyhemoglobin	Iso	Hypo
Early Subacute	3 - 7 days	Methemoglobin in RBCs	Hyper	Hypo
Late Subacute	> 7 days	Methemoglobin Free	Hyper	Hyper
Chronic	> 14 days	Hemosiderin	Iso, Hypo	Hypo

intracellular
extracellular

<http://emedicine.medscape.com/article/344973-overview>
<http://radiologymri.blogspot.tw/2010/12/intracranial-hemorrhage-on-mri.html>

