



磁振影像學MRI

磁振假影

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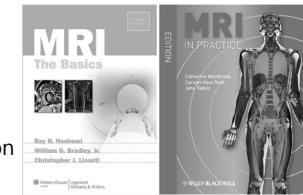
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本週課程內容 <http://cflu.lab.nycu.edu.tw>

- 磁振假影

- MRI The Basics (3rd edition)
 - Chapter 18: Artifacts in MRI
- MRI in Practice, (4th edition)
 - Chapter 7: Artefacts and their compensation



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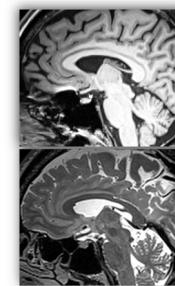
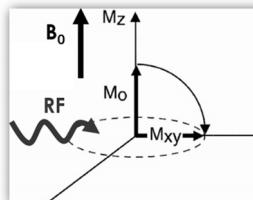
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Procedure of MRI

- Alignment (magnetization) B_0
- Precession $\omega_0 = \gamma B_0$
- Resonance (given B_1 by RF with ω_2) $\omega_1 = \gamma B_1$, $\omega_1 \perp \omega_0$
 - The most effective resonance is produced when $\omega_0 = \omega_2$
- MR signal (EMF, relaxation time)
- Imaging (Pulse sequencing: SE, GRE, EPI)
 - Tissue Contrast: Image weighting
 - Spatial localization: Slice selection & Spatial Encoding
 - Data space/K space
- Tissue Suppression Techniques
- Artifacts in MRI



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磁振假影

Artifacts in MRI

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Hardware-related Artifacts

- Radio frequency (RF)-related artifact
 - Cross-talk
 - Zipper artifacts
- External magnetic field artifacts
 - Magnetic inhomogeneity
- Gradient-related artifacts
 - Eddy currents
 - Nonlinearity
 - Geometric distortion

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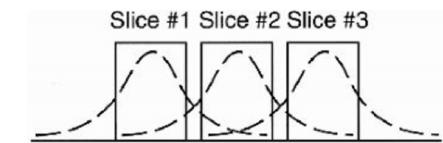
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RF-related artifacts: Cross talk

- An imperfect rectangle of the FT of the RF pulse
- Decrease TR due to saturation of protons by the RF for adjacent slices.
- T1 weighting ↑ and SNR ↓
- Remedy: interleaving, increase gap, rectangular wave



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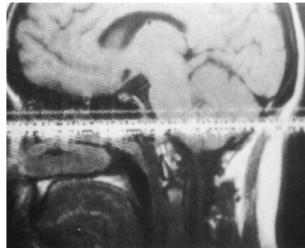
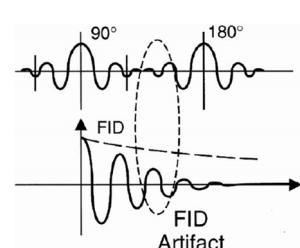
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RF-related artifacts: Zipper artifacts

- Along the phase encoding axis at zero frequency
 - Cause 1, RF feed-through: excitation RF pulse → receiver coil
- Along the frequency-encoding axis without phase encoded
 - Cause 2, Stimulated echo: imperfect RF pulses of adjacent slices, imperfect 90° - 180° - 180° pulses
 - Cause 3, FID artifact: the overlapping of 180° RF pulse with the FID



Central artifacts

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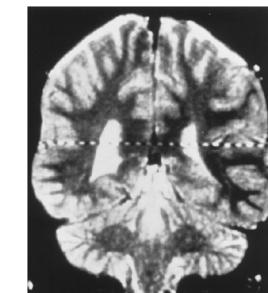
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RF-related artifacts: Zipper artifacts

- Remedy to FID artifact:
 - Increase TE (increase the separation between FID and RF pulse)
 - Increase slice thickness (a wide RF BW narrows RF signal in the time domain)
- Remedy to stimulated echo:
 - Use spoiler gradients
 - Adjust the transmitter



Central artifacts

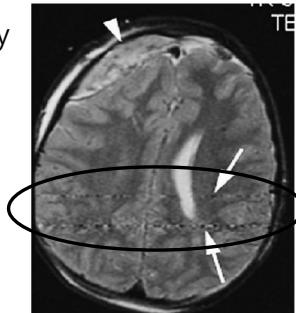
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RF-related artifacts: Zipper artifacts

- Unwanted external RF noise (TV, radio station, electronic monitoring equipment)
- Occurs at the specific frequency
- Remedy: improve RF building, shut the door of MR room



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External magnetic field artifacts

- Improper shimming, environmental factors, far extremes of short bore magnets

- Remedy: auto shimming



Moiré fringes (zebra pattern)

T2 fat-suppressed image

Upper slice

Lower slice

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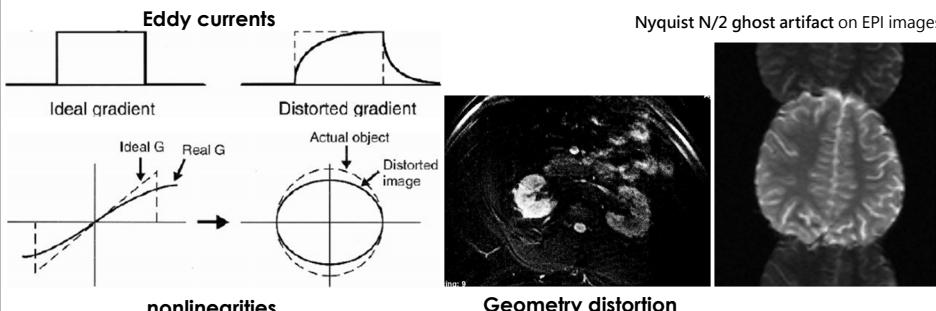
T1 image



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Gradient-related artifacts

- Eddy currents are generated when the gradients are rapidly switched on and off, resulting in a distortion in the gradient profile.



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Software-related Artifacts

- Image processing artifact
 - Aliasing
 - Chemical shift
 - Truncation
 - Partial volume



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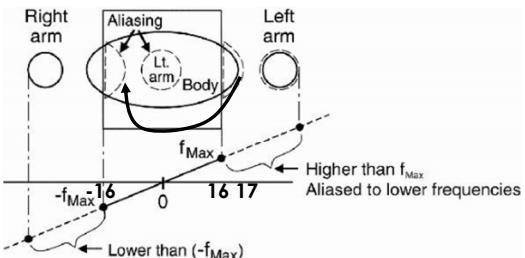
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Image processing Artifacts: aliasing

- Any frequency higher than the maximum frequency allowed by the gradient cannot be detected correctly.
- $f(\text{perceived}) = f(\text{true}) - 2f(\text{max})$



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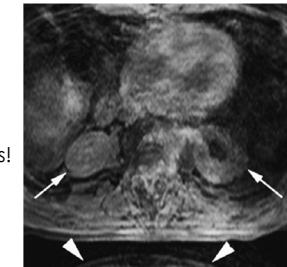
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Image processing Artifacts: aliasing

- 2D imaging: along frequency-encoding or phase-encoding directions
- 3D imaging: in all three directions

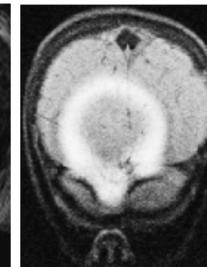
3D axial imaging



Kidneys in lungs!

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3D coronal imaging



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Image processing Artifacts: aliasing

- Remedy
 - Increase FOV (may reduce spatial resolution)
 - Use surface coils that only covers the area within FOV.
 - Frequency or phase oversampling ("No Phase Wrap")
 - Use saturation pulses to saturate the signals outside the FOV.

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Image processing Artifacts: chemical shift

- The protons from different molecules precess at slightly different frequencies.
- The protons in H_2O precess slightly faster than those in fat (about 3.4 ppm).
- $\omega_0 = \gamma B_0 = (42.6 \text{ MHz/T})(1.5\text{T}) = 64 \text{ MHz}$
- $64 \text{ MHz} \times 3.4 \text{ ppm} = (64 \times 10^6 \text{ Hz})(3.4 \times 10^{-6}) \approx 220 \text{ Hz}$
- $B_0 \uparrow$, chemical shift \uparrow

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Image processing Artifacts: chemical shift

- BW = $N_x/T_s = 256/(8 \text{ ms}) = 32 \text{ kHz}$
- BW/pixel = $1/T_s = 125 \text{ Hz}$
- Pixel difference ($\text{H}_2\text{O}/\text{fat}$) = $220 \text{ Hz} / 125\text{Hz} = 1.76 \text{ pixels}$
- Fat protons are going to be misregistered from H_2O by about 2 pixels (in a 1.5 T magnet using a standard 32kHz bandwidth).
- $\text{chemical shift (in mm)} = \frac{3.5 \times 10^{-6} \mu\text{B}_0 \times \text{FOV}}{\text{BW}}$

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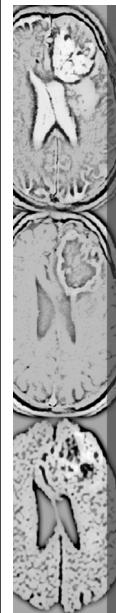


Image processing Artifacts: chemical shift

- Chemical shift artifact only occurs in the frequency-encoding direction.
 - A bright band toward the lower frequencies
 - A dark band toward the higher frequencies



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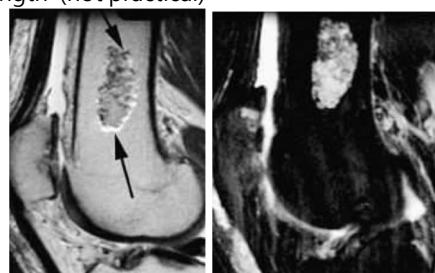
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Image processing Artifacts: chemical shift

- Remedy:
 - Fat suppression
 - Increase pixel size by keeping FOV the same and decreasing Nx (spatial resolution \downarrow)
 - Lower the magnet's field strength (not practical)
 - Increase bandwidth (SNR \downarrow)
 - Use a long TE (less signal from fat)

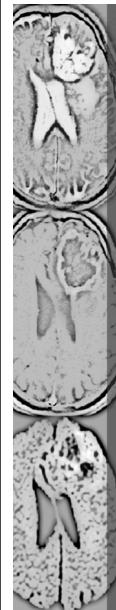


T2 with/without fat saturation

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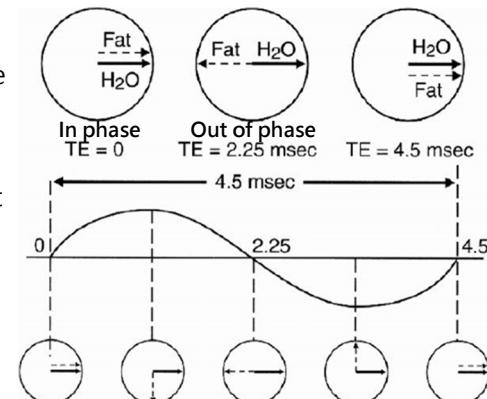
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Chemical shift of the second kind

- 220 Hz at 1.5T:
- Fat and water are in phase every 4.5 msec.
- Only exist in GRE (without 180° rephasing pulse).
- Not only in the frequency-encoding direction



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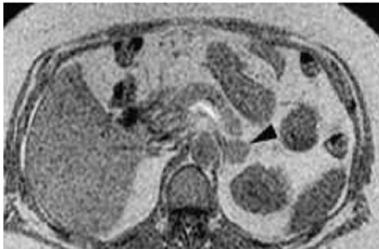
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Chemical shift of the second kind

- Boundary effect (when out of phase)

In phase



Out of phase



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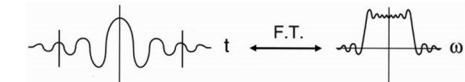
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Image processing Artifacts: Truncation

- Truncation artifacts (Gibbs Phenomenon)
- Occurs at high contrast interfaces
 - Skull/brain, spinal cord/CSF, meniscus/fluid in the knee
- Due to insufficient samples for the large signal changes
 - Mostly seen in the phase direction (because fewer samples are usually taken)
- Causes alternating bright and dark bands
 - Pseudo syrinx of the spinal cord
 - Pseudo tear of the knee meniscus

The K-space data is often under-sampled and truncated to shorten the scan time.



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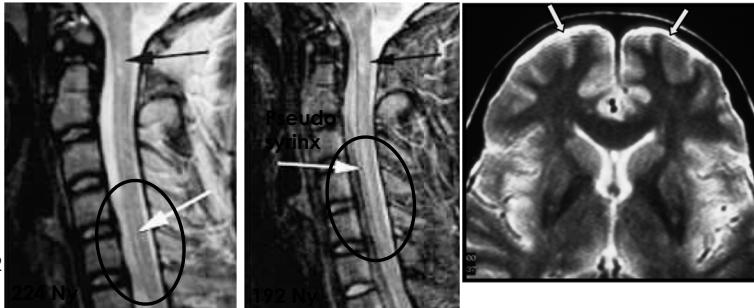
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Image processing Artifacts: Truncation

- Remedy:

- Decrease pixel size (increase phase encoding steps, reduce FOV)
- Increase sampling time, increase sampling bandwidth



Fat-saturated T2

1224 NY

192 NY

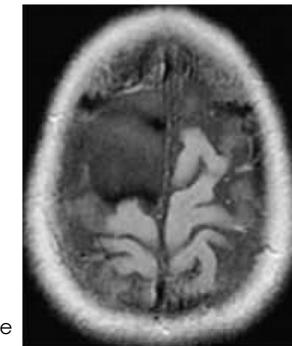
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Image processing Artifacts: Partial volume

- Remedy: decrease the slice thickness



Axial FLAIR image

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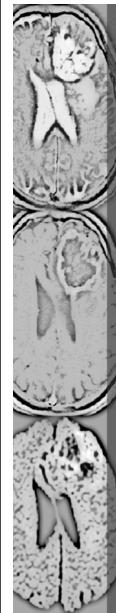
Subject-related Artifacts

- Motion artifacts
- Magnetic susceptibility artifacts
 - Diamagnetic, paramagnetic, ferromagnetic
 - Metal

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Subject-related Artifacts: Motion

- Random movements, periodic motion (pulsating flow in vessels)
- We only get motion artifacts in the phase-encoding direction (the sampling time for frequency-encoding is short).

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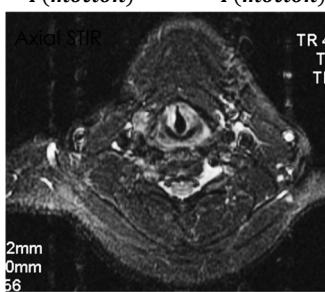
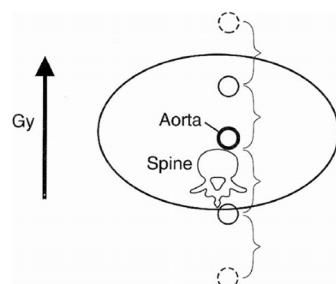
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Periodic Motion

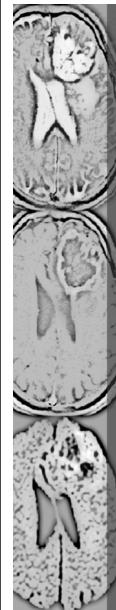
- Ghost artifacts of the vessels are equally separated along phase-encoding direction.
- **separation (SEP in pixels) = $\frac{TR \times Ny \times NEX}{T(motion)} = \frac{\text{acquisition time}}{T(motion)}$**



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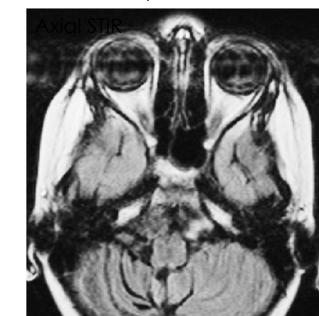
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Motion artifacts

- Remedy for Periodic motion
 - Spatial presaturation pulses to saturate inflowing protons
 - Increase separation between ghosts
 - Swap phase and frequency (only change the direction of artifacts)
 - Use cardiac/respiration gating
 - Use flow compensation
- Remedy for random motion
 - Patient instruction: **don't move!**
 - Fast scanning techniques
 - Sedation

Random eye movements

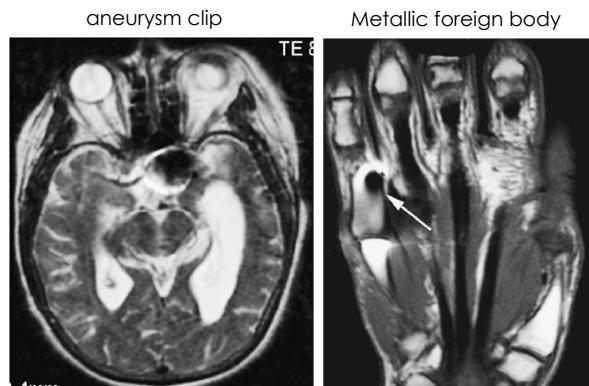


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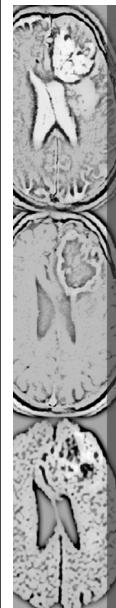
Magnetic susceptibility artifacts



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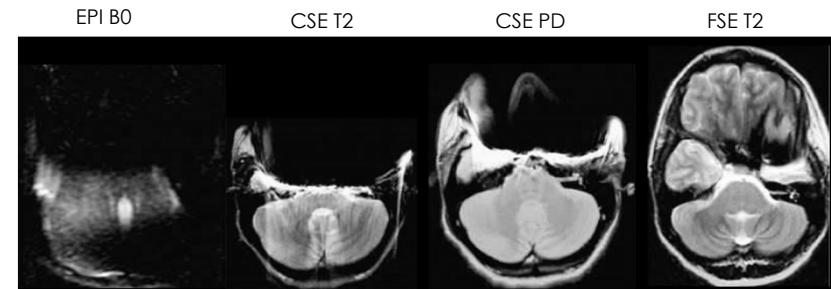
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Magnetic susceptibility artifacts

- A patient with dental braces



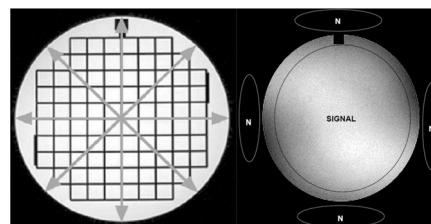
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- 請完整練習此部分國考題，很多臨床假影影像實例！
- 請務必閱讀ACR MRI phantom (11 slices)補充教材！

<補充資料>
[ACR phantom overview.pdf](#)
[ACR phantom guidance.pdf](#)
[ACR 官網連結](#)



- Geometric Distortion
- Spatial Resolution
- Slice thickness and position
- Interslice Gap
- Estimate of Image Bandwidth
- Low Contrast Detectability
- Image Uniformity
- Signal-to-Noise Ratio (SNR)
- Physical and Electronic Slice Offset
- Landmark

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THE END

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