

Magnetic Resonance in Medicine Course Introduction & Principle Review

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Congratulations!

- You are HERE!



License of
Radiological Technologist



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Syllabus

- 1 Course Overview & Review of MRI basic principles
- 2 Diffusion weighted imaging (DWI)
- 3 Diffusion tensor imaging (DTI) & tractography
- 4 MR angiography
- 5 MR contrast agent
- 6 MR perfusion: DCE & DSC
- 7 MR perfusion: arterial spin labeling (ASL)
- 8 Susceptibility weighted imaging (SWI)
- 9 (4/15) MRI Examination Procedure
- 10 (4/22) Yang-Ming 3T MRI room visiting and scanning
- 11 Functional MRI (fMRI) I
- 12 (5/6) Functional MRI (fMRI) II (online video)
- 13 MR Spectroscopy (MRS)
- 14 Cardiac MR imaging
- 15 MR muscle skeleton imaging
- 16 (6/3) Final Competition
- 17 端午節放假
- 18 Literature survey: MRI clinical research

<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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Evaluation

- Attendance & participation in class activities (40%)
- 3T MRI visiting (30%)
- Final exam (30%)
 - Group competition.

<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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From Basics to Bedside

- **Magnetic Resonance Imaging 磁振影像學**

http://cflu.lab.nycu.edu.tw/CFLu_course_BIRSmri.html

Principles of MRI

Equipment, pulse sequence, tissue contrast, image reconstruction, MRI artifacts, safety issues

- **Magnetic Resonance in Medicine 醫用磁振學**

http://cflu.lab.nycu.edu.tw/CFLu_course_BIRSmrm.html

Clinical Applications of MRI

MR contrast agent, functional MRI, diffusion weighted imaging, angiography, MR spectroscopy

Visiting NYCU 3T MRI Facility



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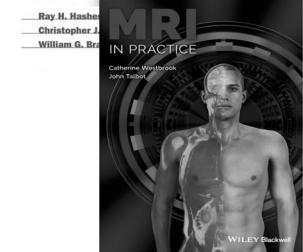
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Textbooks

- **MRI The Basics (4th edition)**

- Ray H. Hashemi, William G. Bradley, Christopher J. Lisanti
- Lippincott Williams & Wilkins, 2017



- **MRI in Practice, (5th edition)**

- Catherine Westbrook, Carolyn Kaut Roth, John Talbot
- Wiley Blackwell, 2018

<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

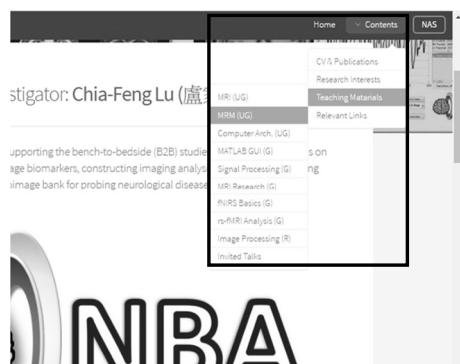
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Online Learning Materials

- Review/Overview/Self Learning

- <http://cflu.lab.nycu.edu.tw>
Teaching Materials → MRM(UG)

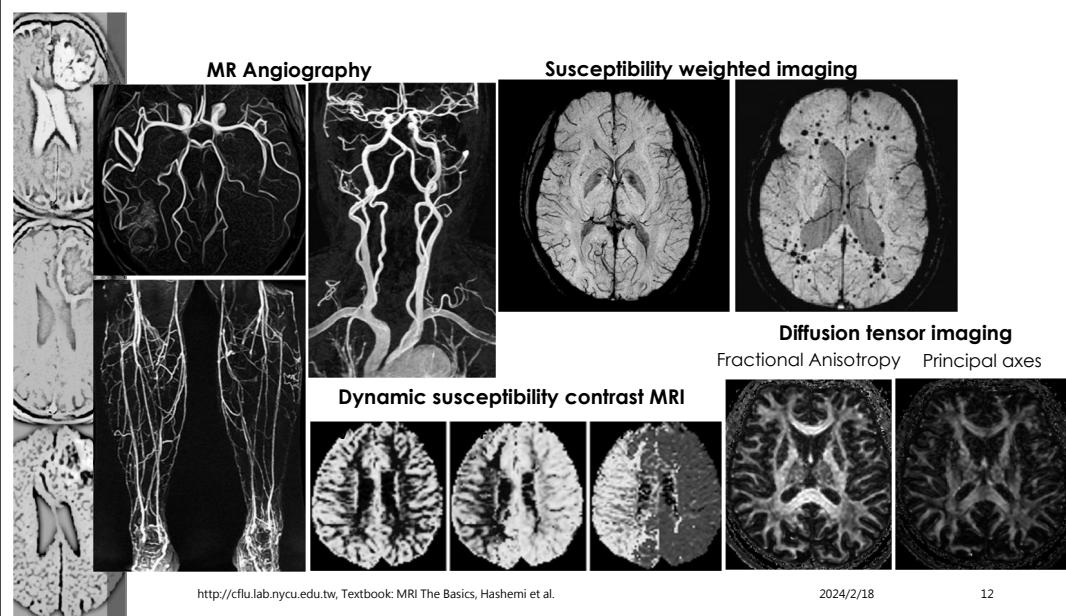


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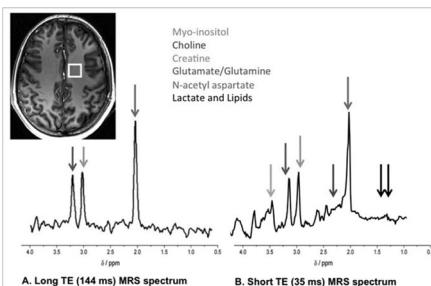
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MR spectroscopy

http://www.massgeneral.org/imaging/news/radrounds/july_2012/

Metabolite	Major resonance (ppm)	Significance	Visible only at short TE	Disease	Metabolic Changes
Lipids (Lip)	0.8±1.4	Breakdown of tissue	Y	Brain tumors	Cho↑, NAA↑, Cr↑, Lac and Lip↑
Lactate (Lac)	1.3	Marker of anaerobic glycolysis	N	Stroke	Lac↑, NAA↑, Glx↑, Cr↑, Cho↑
NAA	2.0	Marker of neuronal health	N	Epilepsy	NAA↑, Lac↑
Glutamate & Glutamine (Glx)	2.1±2.6	Excitatory neurotransmitter	Y	Multiple sclerosis	NAA↑, Cho↑, (Cr↑)
Cho	3.2	Marker of membrane metabolism, cell proliferation	N	HIV/AIDS	NAA↑, Cho↑, MI↑
Cr	3.0 (and 3.9)	Marker of cellular energetics	N	Traumatic Brain Injury	NAA↑, Cho↑, Lac↑
Myo-inositol (MI)	3.5	Osmolytic marker; proposed glial marker	Y	Heaptic Encephalopathy	Cho↑, MI↑, Glx↑
				Hypoxic Ischemic Injury	Lac↑, NAA↑, Glx↑, Cr↑
				Neurodegenerative diseases	
				Alzheimer	NAA↑, MI↑
				Parkinson	NAA↑ (Striatum)
				Huntington	NAA↑, Cho↑ (Basal ganglia)
				ALS	NAA↑ (Motor cortex, Brain stem)

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Review Materials of MRI Principles

磁振造影原理複習教材

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Let's Review What We Have Learned!

https://miro.com/app/board/uXjVNrz9yO0/?share_link_id=413130478279



miro



Using App or Chrome

Password: ilovemri

<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

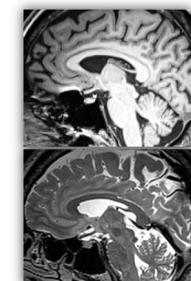
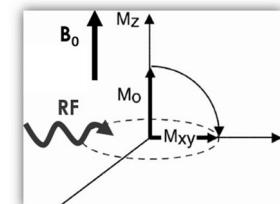
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Procedure of MRI

- Alignment (magnetization) B_0
- Precession $\omega_0 = \gamma B_0$
- Resonance (given B_1 by RF with ω_2) $\omega_1 = \gamma B_1$, $B_1 \perp B_0$
 - The most effective resonance is produced when $\omega_0 = \omega_2$
- MR signal (EMF, relaxation time)
- Imaging (Pulse sequencing: SE, GRE, EPI)
 - Tissue Contrast: Image weighting
 - Spatial localization: Slice selection & Spatial Encoding
 - Data space/K space
- Tissue Suppression Techniques
- MR artifacts and safety issues

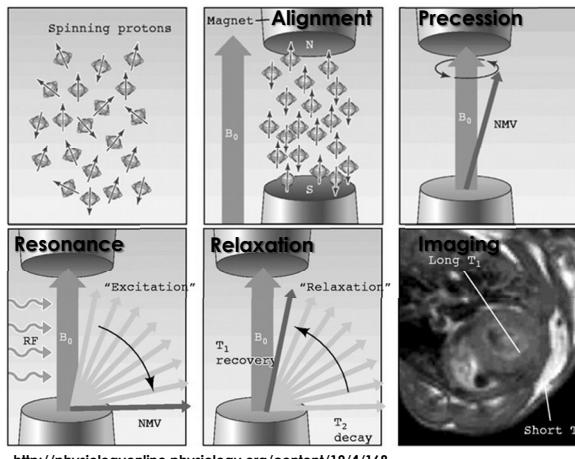


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Principles of MR imaging



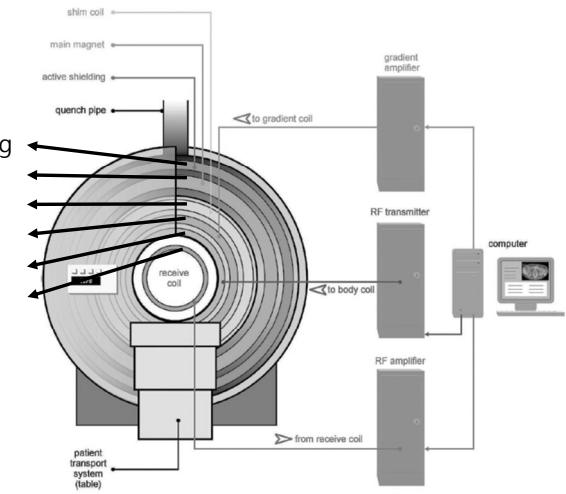
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Setup

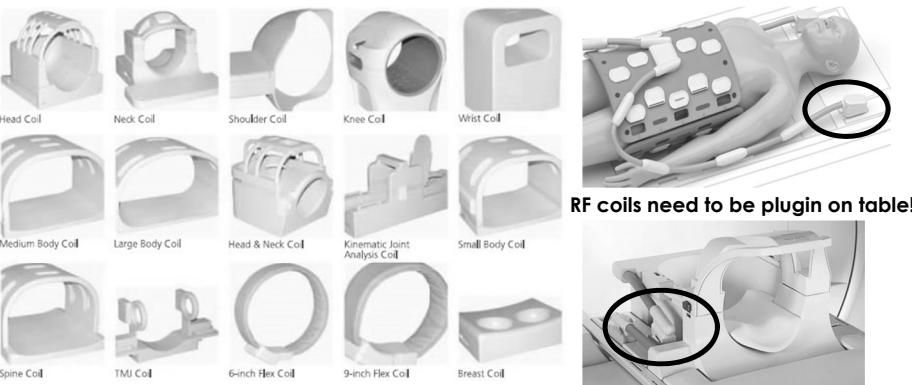
- Outer → inner
 - Active shielding
 - Main magnet
 - Shim coil
 - Gradient coil
 - Body coil
 - Receive coil



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RF Coil Shapes



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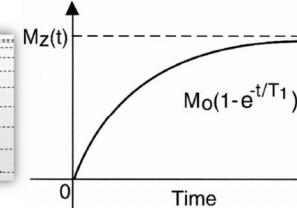
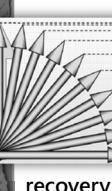
T1 & T2 Relaxation Time

T1:
The longitudinal relaxation time
The spin-lattice relaxation time

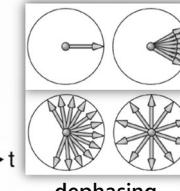
$$M_z(t) = M_0(1 - e^{-t/T_1})$$

T2:
The transverse relaxation time
The spin-spin relaxation time

$$M_{xy}(t) = M_0 e^{-t/T_2}$$



$T_1 > T_2 > T_2^*$



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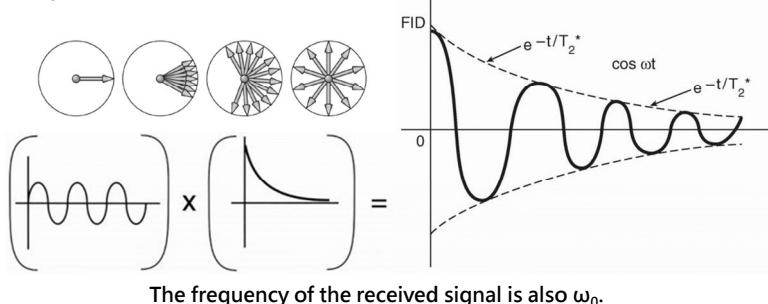
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Received Signal: Free Induction Decay

- The oscillating, decaying signal is called an FID.
- $M_{xy}(t) = M_0 e^{-t/T_2^*} (\cos \omega_0 t)$



<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

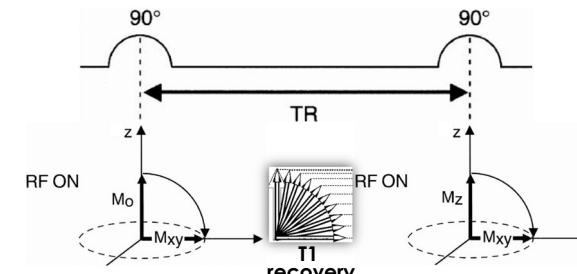
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TR (Repetition Time)

- To spatially encode the signal and to increase the signal-to-noise ratio, we have to apply the RF pulse *multiple times* while varying the gradients.
- The time interval between RF pulses is called TR.



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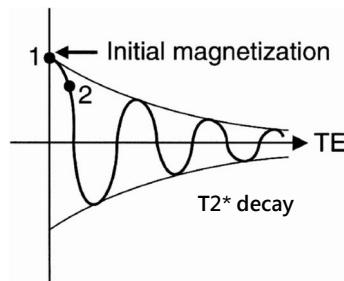
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TE (Time to Echo or Echo Delay Time)

- We wait a short period of time (TE) after RF pulse and then make the measurement.
- The T2* decay curve (FID) starts out at the value of $M_0(1-e^{-TR/T1})$ on the T1 recovery curve and then decays very quickly.



<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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Image Contrast

- Long TR, short TE \rightarrow proton density
- Long TR, long TE \rightarrow T2*-weighted
- Short TR, short TE \rightarrow T1-weighted
- Short TR, long TE \rightarrow no signal

Example:

Long TR	2000 ms
Short TR	300–700 ms
Long TE	60 ms+
Short TE	10–25 ms

Table 2.3 Parameters used in gradient echo.

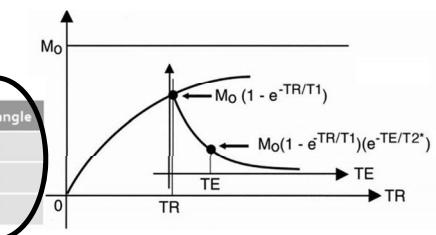
Weighting	TR	TE	Flip angle
T1	short	short	large
T2	long	long	small
Proton density	long	short	small



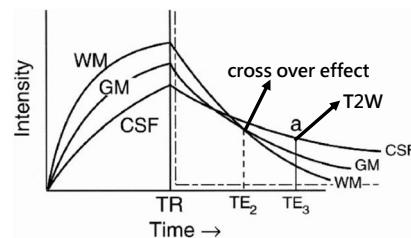
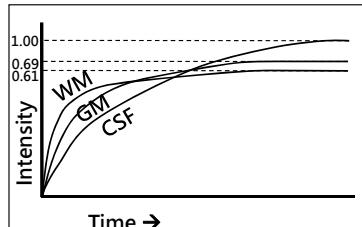
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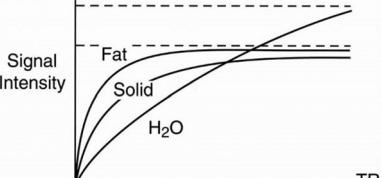


Adjust T1 and T2 weighting



T1: CSF > GM > WM
 T2: CSF > GM > WM
 N(H): CSF > GM > WM

T1: H₂O > Solid tissue > Fat
 T2: H₂O > Fat > Solid tissue
 N(H): H₂O > Fat > Solid tissue



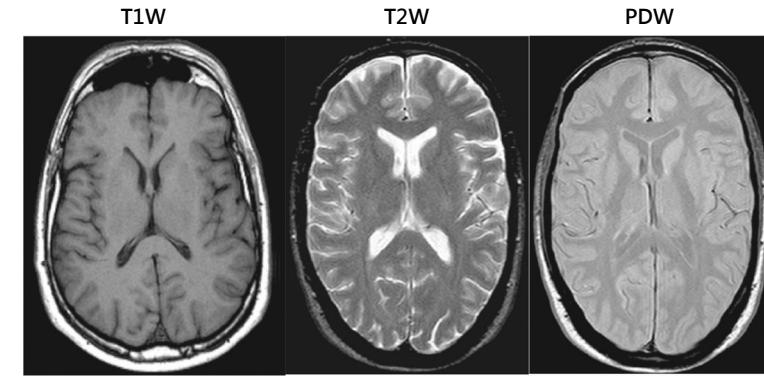
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T1/T2/PD weighted Images



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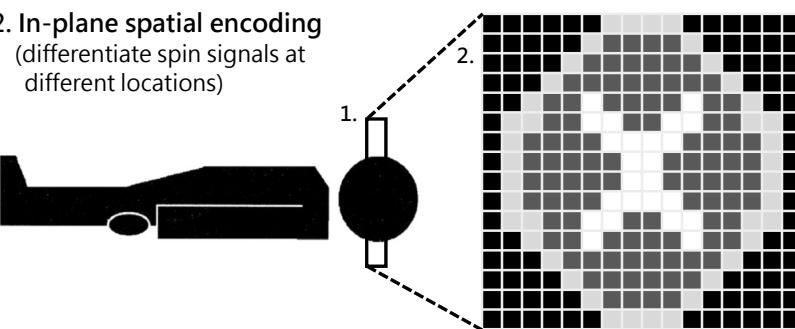
Image Construction

1. Slice selection

(only excite spins on a specific slice location)

2. In-plane spatial encoding

(differentiate spin signals at different locations)



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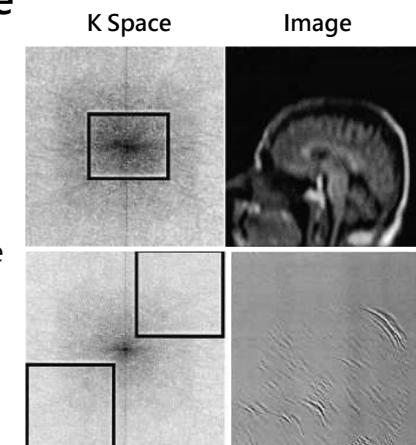
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Image of K-Space

- The center of k-space contributes to the primary information of image.

- The periphery of k-space provides information regarding fitness of the image and clarity at sharp interfaces



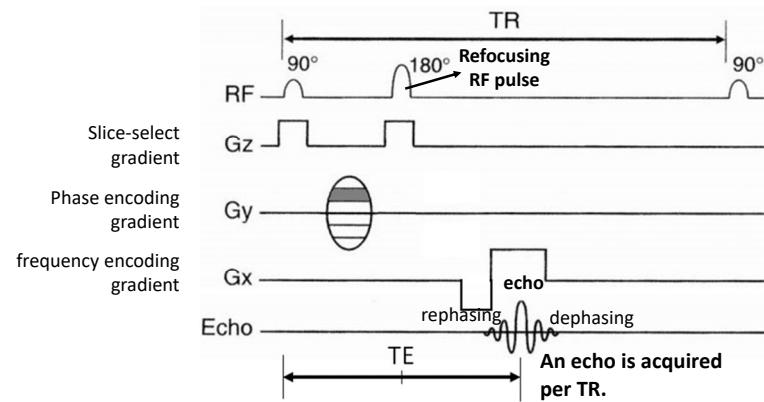
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Spin-echo pulse sequence diagram



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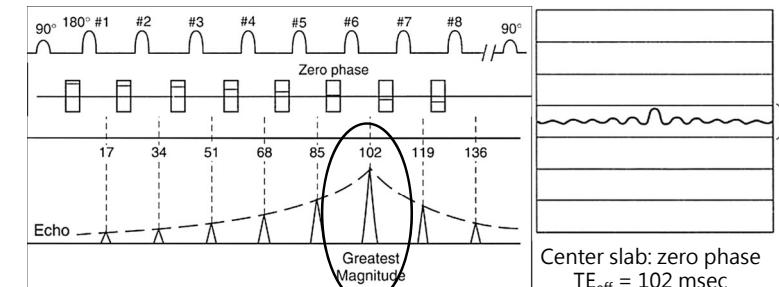
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Fast spin echo

- In FSE, before each 180° pulse, we place a different value of the phase-encoding gradient.
- For the 180° pulse before the echo we choose as the TE_{eff} (in this case, 102 msec), we use a phase-encoding gradient with the lowest strength.



<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

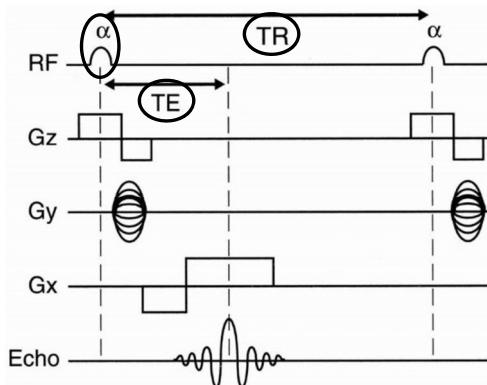
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GRE Pulse Sequence Diagram

- Three operator-controlled parameters that affect the tissue contrast.
- Coherent GRE
- Incoherent GRE



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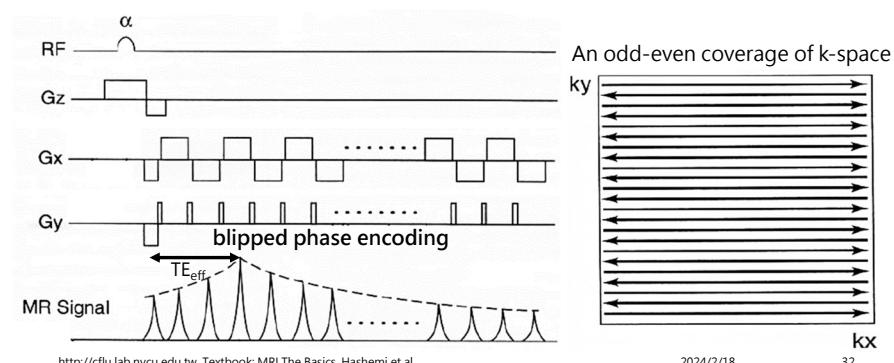
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Single-shot EPI

- The phase-encode gradient is subsequently applied briefly during the time when the readout gradient was zero (200 μ sec).



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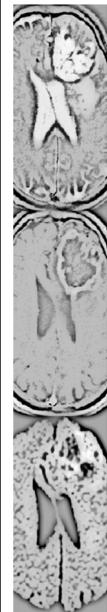
Contrast in EPI

- Contrast in EPI depends on the "root" pulsing sequence
- SE-EPI (90° - 180° -EPI)
- GRE-EPI (α° -EPI)
- IR-EPI (180° - 90° - 180° -EPI)
 - inversion-recovery (IR)

<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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Suppression techniques

- To suppress the signal coming from a certain tissue.
 - Two common targets (tissues): fat and water
- Suppression techniques
 - Inversion recovery (IR) techniques
 - Chemical/spectral saturation
 - Dixon method
 - Spatial presaturation
 - Magnetization transfer (MT)

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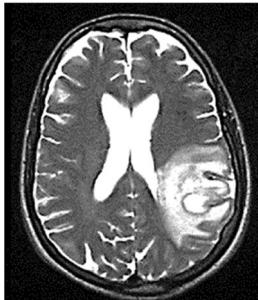
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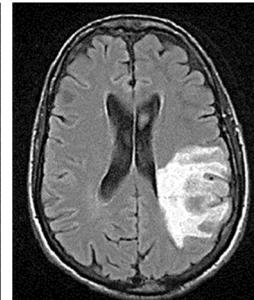
Glioblastoma MRI

T2 Weighted image



<http://journal.frontiersin.org/article/10.3389/fonc.2013.00066/full>

T2 FLAIR (Water suppression)

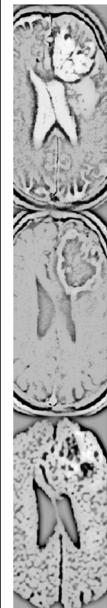


edema vs. water

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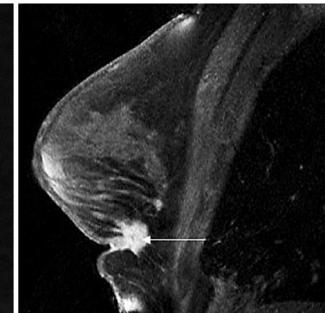
Breast cancer MRI

T1 Weighted image



T1: $H_2O > \text{Solid tissue} > \text{Fat}$
Gd contrast agent can shorten tissue T1

Fat saturation + Gd enhancement



British Journal of Cancer (2003) 88(1), 4-10

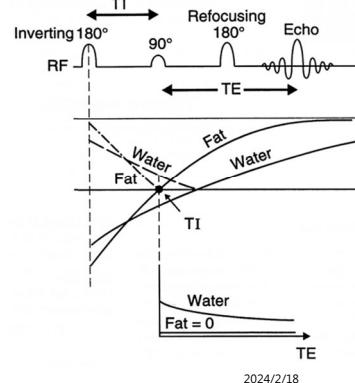
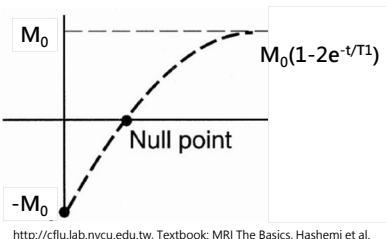
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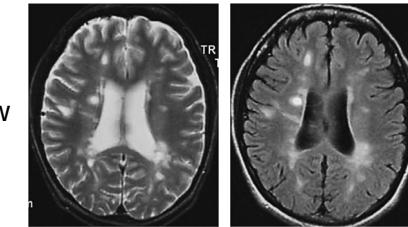
Inversion recovery, IR

- After the 180° RF pulse, the magnetization starts to recover from $-M_0$ instead of zero.
- $TI(\text{null}) = (\ln 2)T1 \approx 0.693 T1$.



Tissue Suppression: STIR & FLAIR

- STIR: Short tau inversion recovery, fat suppression
 - At 1.5T, $TI = 0.693 \times 200 = 138.6$ msec
- FLAIR: Fluid attenuated inversion recovery, water suppression
 - At 1.5T, $TI = 0.693 \times 3600 = 2494.8$ msec



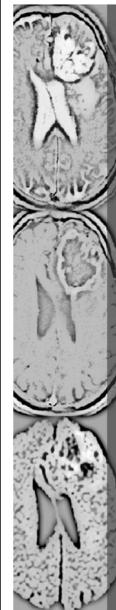
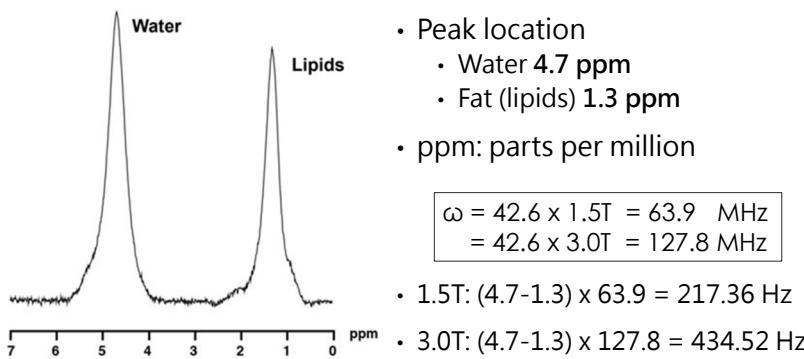
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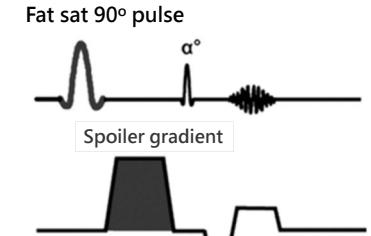


Water & fat chemical shift



Chemical/spectral presaturation

- A frequency-selective presaturation pulse is applied before the RF excitation pulse.
- CHESS: Chemical shift selective
- We select appropriate frequency (based on the Larmor equation) to suppress fat or water.



- At 1.5T, water protons precess 210-220 Hz faster than fat protons;
- At 3.0T, water protons precess 420-440 Hz faster than fat protons.

<http://mri-q.com/fat-sat-pulses.html>

<http://cflu.lab.nycu.edu.tw>, Textbook: MRI The Basics, Hashemi et al.

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THE END

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